Parametric Analysis of Fatigue in Stationary Biking: A Computational Approach

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Introduction

- As personal fitness is increasingly prevalent in society, a focus on maintaining safe exercise technique is crucial in avoiding training injury.
- Stationary biking, or spinning, is an exercise commonly done in large group settings led by an instructor who controls cycling intensity, but does not closely monitor individual technique.
- Over long duration training, fatigue may cause improper cycling form, leading to knee, hip, and back injuries. Performance fatigue research is also applicable to the military, athletics, and clinical rehabilitation

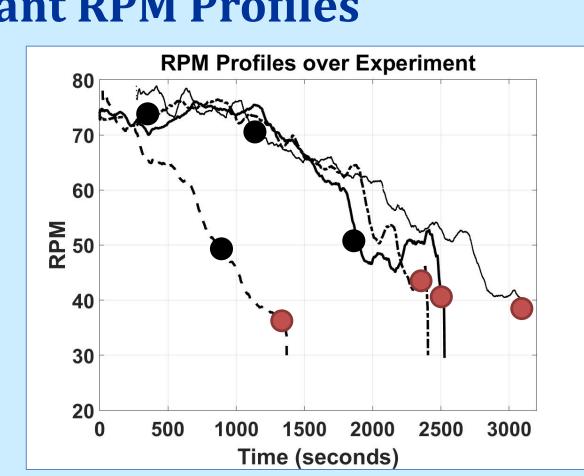
Objectives

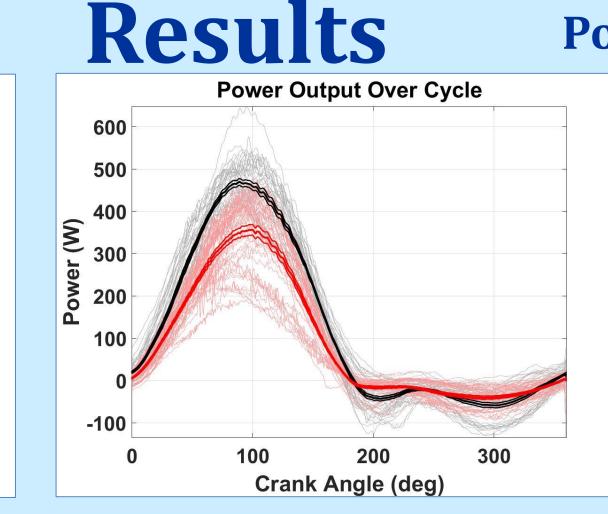
- 1. Develop streamlined protocol for long duration volunteer testing.
- 2. Establish analysis pipeline for post processing of kinematic, kinetic, and physiological data.
- 3. Conduct multi-variate investigation of fatigueinduced performance changes.
- 4. Identify volunteer parameters potentially linked to the fatigue process.

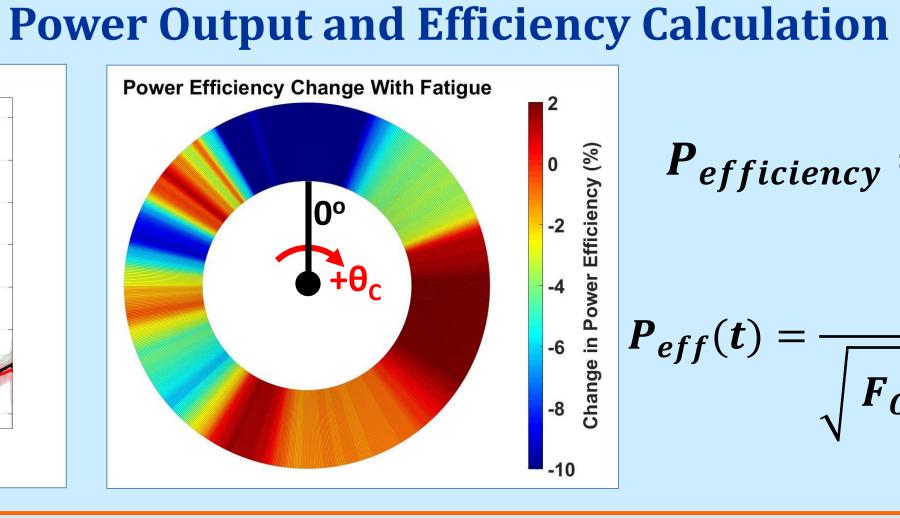
Methods **Data Collection Methods Data Collection Pedal/Seat Load Cells Motion Capture System** 11 EMGs, 1 EKG 65 Markers, 9 Cameras & Velocity Gate **Data Processing Power Calculation EMG Filtering** 60 Hz 4° Notch Work Force * Distance Time 30-300Hz 4° BPF Assuming Work to Rotate Pedal ≈ 0, **De-Mean** $P_{avg}(t) = \frac{\frac{1}{2}[F_{Cz}(t-1) + F_{Cz}(t)] * \|\overrightarrow{R}\|}{\Delta t}$ Rectify 20Hz 4° LPF Inverse Inverse **OpenSim Analyses** Scaling Model Generic **Subject-Specific Kinematics Dynamics** Joint Muscle **Kinematics** Forces Model Model **Definitions** Marker Set **Marker Set Boundary Reaction Forces** & Constraints for $t = 0 \rightarrow end$ @ Seat and Pedals @ t = 0Computed Muscle Control **OpenSim Analysis Pipeline** Analyze Secondary **Optimized Muscle Activation,** OpenSim User **OpenSim Process Outputs Refined Kinetics & Kinematics Variables**

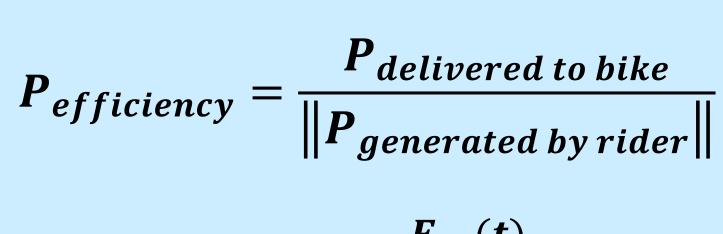
Guided and Resultant RPM Profiles

Guided Endurance Routine		
Duration	Resistance	Target RPM
2.5 minutes	Low	60-75
2.5 minutes	Medium	60-75
2.5 minutes	High	60-75
Maintain**	High	60-75

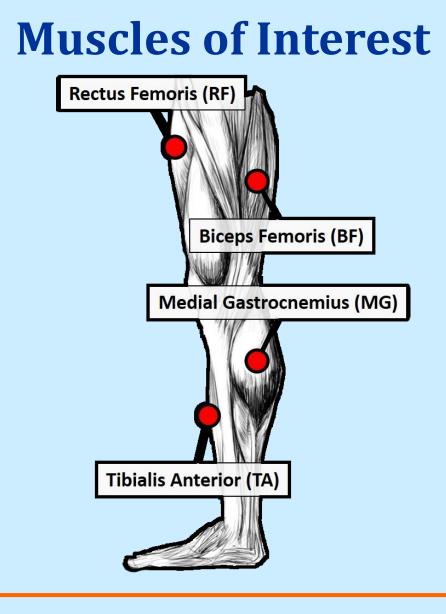






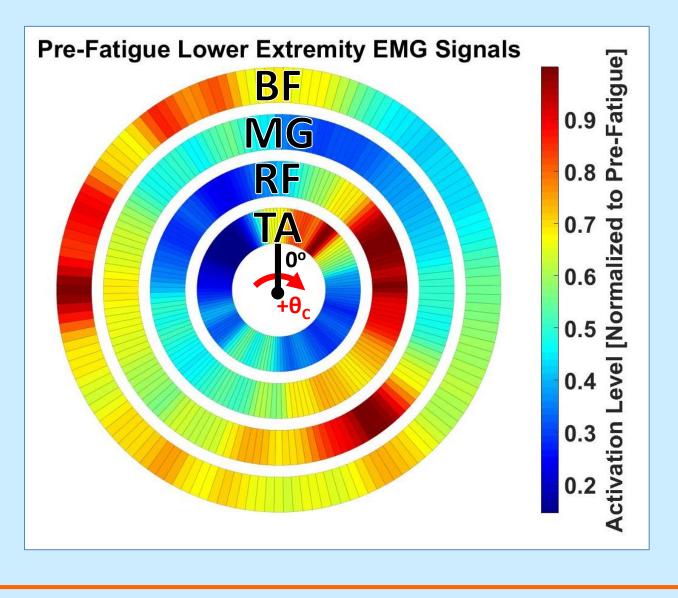


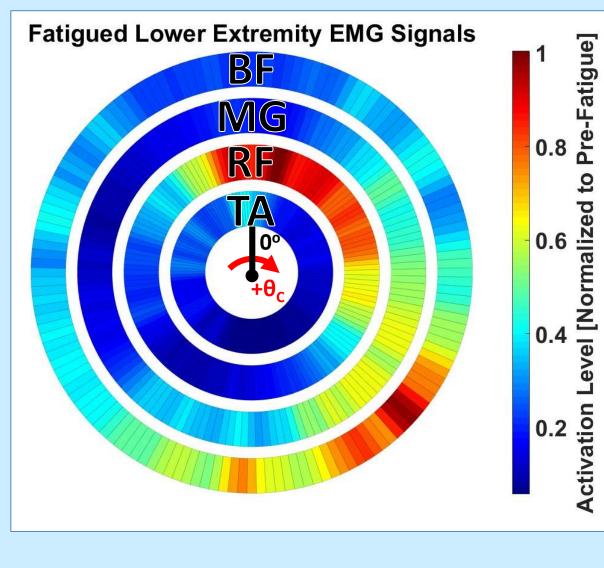
$$P_{eff}(t) = \frac{F_{Cz}(t)}{\sqrt{F_{Cx}(t)^2 + F_{Cy}(t)^2 + F_{Cz}(t)^2}}$$

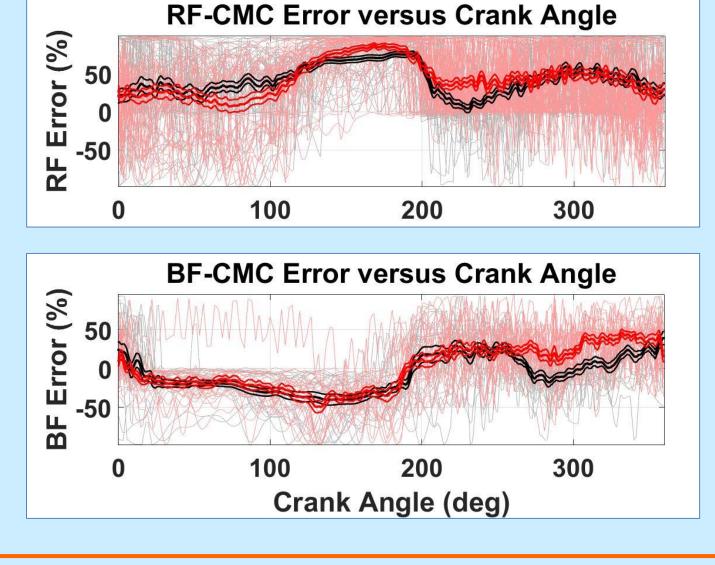


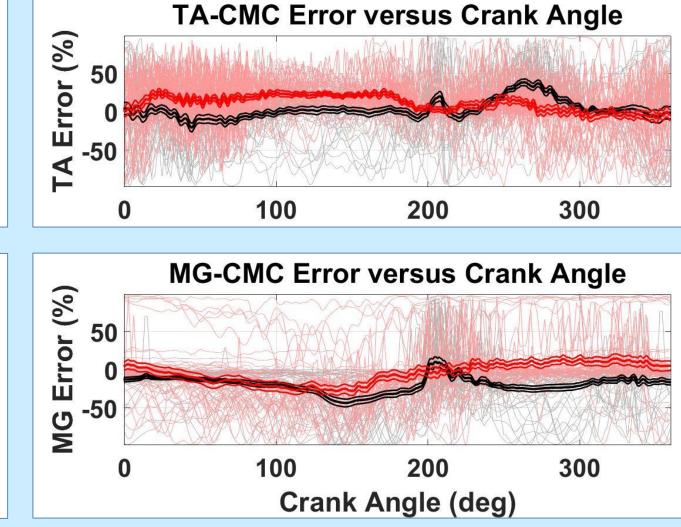
Kinetics

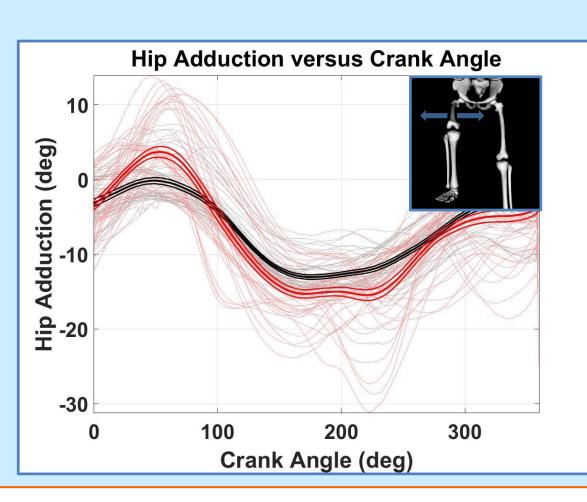
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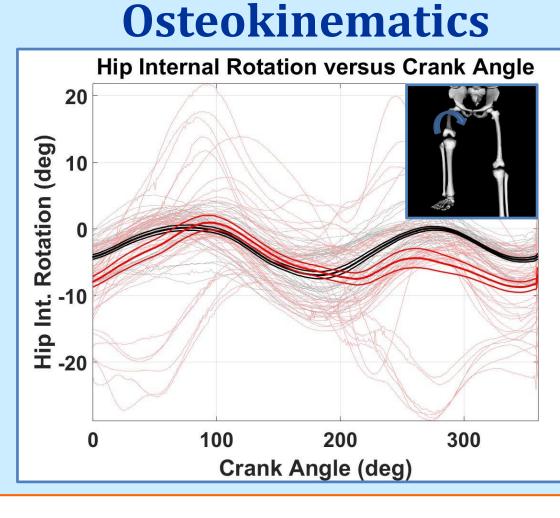


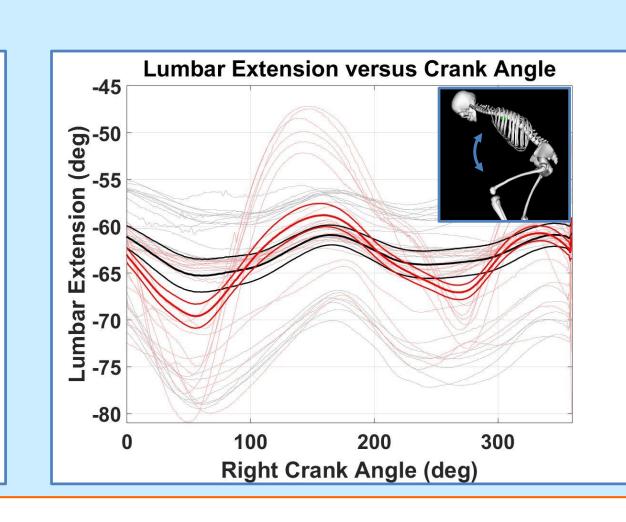


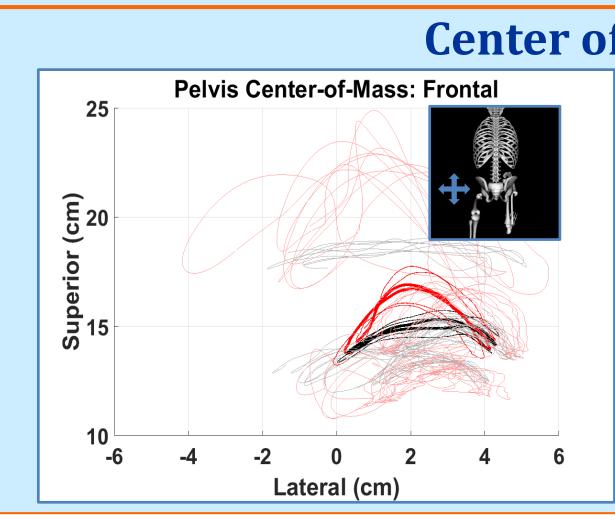


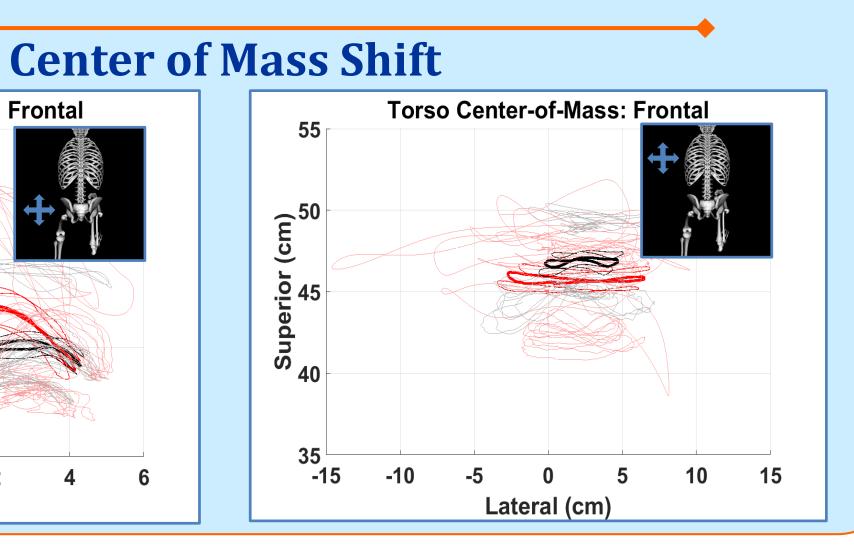












Discussion

- Four of the thirteen subjects exhibited uniform fatigue during their test, characterized by: decreased net power output, increased kinetic variability, and slightly decreased power efficiency.
- * Physiological changes were seen bilaterally in parallel with kinetic performance reduction, such as: loss of tibialis anterior activation on the down stroke, duration decrease and amplitude increase of the rectus/biceps femoris.
- * Computational prediction of muscle activation shows large deviations from experimentally observed muscle activation patterns. Such incongruences of the data could be attributed to the noise associated with EMGs or error propagations commonly seen in computational modeling.
- Steokinematic variability in the hips and lower back indicate increased mediolateral knee sway, hip external rotation, and lumbar flexion. Center of mass tracking of the pelvis demonstrates anterior excursion, while the torso indicates increased lateral sway. Further statistical analyses are necessary for fatigue model development.

Acknowledgements

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