

A Preliminary Step Towards a Calvarium Surrogate Model to Simulate Fracture

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1. Introduction

- Surrogate head models are composed of rigid-based material to achieve repeatable head-kinematic and brain responses [1-2].
- These models are effective for helmet assessment and quantifying injurious scenarios but cannot mimic a skull fracture.
- Skull fractures are life-threatening and are observed in contact sports, physical assaults, and vehicle accidents [3]. Thus, we must work towards the development of surrogates of the skull to model fracture.
- Validated skull models can be integrated with existing head forms to mimic and observe fractures and then assess strategies to prevent skull fractures.

2. Objectives

- Introduce the preliminary design of a layered beam calvarium surrogate to model fracture.
- The surrogate's stress and strain measurements at fracture were then compared against human calvarium in quasi-static 4-point bending.

3. Methods

3.1 Fabrication

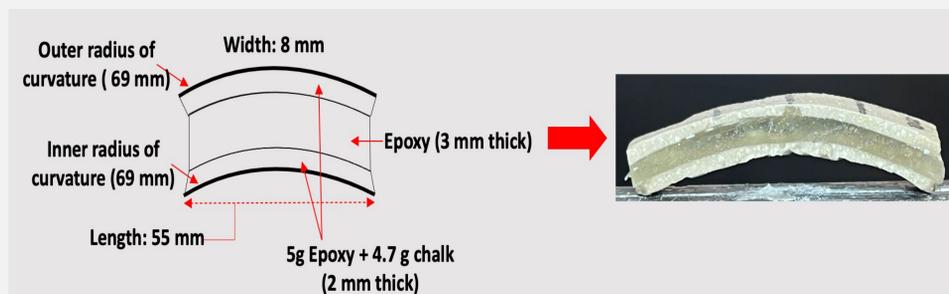


Figure 1. A schematic (left) and photo image (right) of the surrogate model.

- Lepage Speed Set Epoxy and powdered chalk were used to fabricate the surrogate (Fig 1).
- Epoxy and chalk were chosen to form rigidity and to induce brittleness in the surrogate, respectively.
- Each layer (3) of the surrogate was fabricated and cured separately for 10 minutes in a silicone mold.
- The layers were then glued together using epoxy and cured for two weeks at room temperature (20–22 °C or 68–72 °F) prior to mechanical experiments.

3.2 Mechanical Experiments

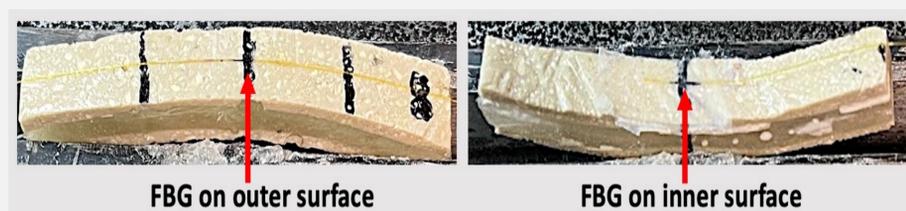


Figure 2. Optical FBGs on the outer and inner surfaces of the surrogate model.

- Each surrogate (n=5) was bonded with optical fibre Bragg gratings (FBGs) to quantify surface strains (%) (Fig 2).

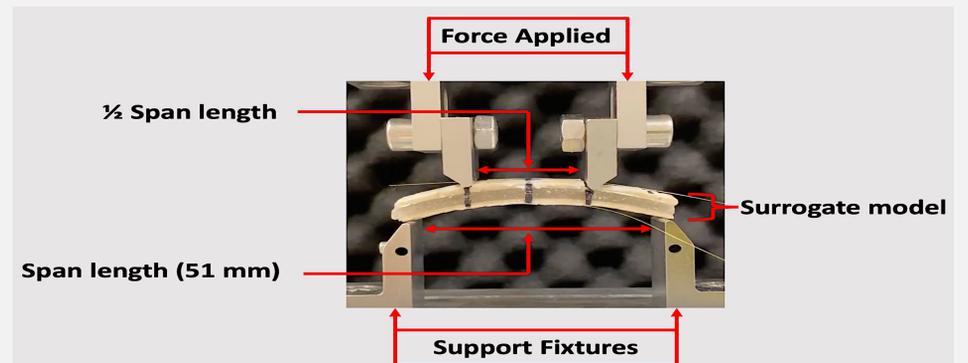


Figure 3. The four-point bending of a surrogate model in an Instron E300

- The surrogates underwent quasi-static 4-point bending (Fig 3) at a displacement rate of 2 mm/min until surrogate fracture.
- Stress was computed using the Euler-Bernoulli beam theorem.
- Stress and strain at fracture were compared between the surrogates and human calvaria (n=5).

4. Results and Discussion

- The average stress and strain at fracture of the surrogate model are close to one SD of the calvarias' mean (Fig 4).
- The surrogates fractured in a brittle manner as observed for calvaria.
- The flexural strength of skull simulants made of fibre-filled (210 MPa) and construction-based (60 MPa) epoxy was reported [4] but greater compared to our surrogates (17.15 MPa) and calvaria (30.13 MPa).

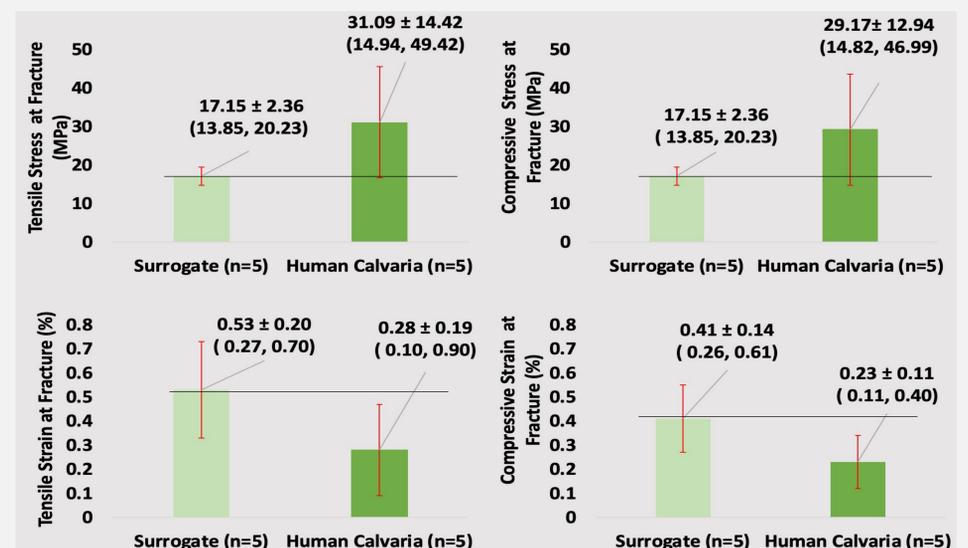


Figure 4. Mean ± standard deviation (SD) (minimum value, maximum value) of stress and strain at fracture between the surrogate and calvaria.

5. Conclusion and Ongoing Work

- Our surrogate model has the potential to model a skull fracture.
- Additional testing on surrogates and calvaria to perform statistical comparisons is ongoing.
- We are testing the surrogate in dynamic impact bending conditions so that the model's mechanical measurements at fracture are valid for strain rates applicable to real-world head impacts.

References

1. Li et al. *J Biomech Eng.* (2021) doi: 10.1115/1.4050752
2. Crandall et al. *Clin Anat.* (2011) doi: 10.1002/ca.21152
3. Yang et al. *Biomed. Res. Int.* (2014) doi: 10.1155/2014/408278
4. Falland-Cheung et al. *J Mech Biomed Mater.* (2017) doi: 10.1016/j.jmbbm.2017.02.023

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